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Structure and function of adsorbed hemoglobin on silica nanoparticles: relationship between the adsorption process and the oxygen binding properties

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KEYWORDS: Adsorption; porcine hemoglobin; silica nanoparticles; protein structure; oxygenation; cooperativity.

ABSTRACT. The connection between the mechanisms of protein adsorption on nanoparticles and the structural and functional properties of the adsorbed protein often remains unclear. We investigate porcine hemoglobin adsorption on silica nanoparticles and we analyze the structural and functional modifications of adsorbed hemoglobin by UV-vis spectrophotometry, circular dichroism and oxygen binding measurement. The structural analysis of adsorbed hemoglobin on silica nanoparticles reveals a significant loss of secondary structure and a preservation of the heme electronic structure. However, adsorbed hemoglobin retains its quaternary structure and exhibits an enhanced oxygen affinity with cooperative binding. Moreover, the structural and functional modifications are fully reversible after complete desorption from silica nanoparticles at pH 8.7. The tunable adsorption and desorption of hemoglobin on SNPs with pH change, and
the full control of hemoglobin activity by pH, temperature and the addition of inorganic phosphate effectors opens the way to an interesting system whereby protein adsorption on nanoparticles can allow for full control over hemoglobin oxygen binding activity. Our results suggest that adsorption of hemoglobin on silica nanoparticles leads to a new structural, functional and dynamic state with full reversibility in a way that significantly differs from protein denaturation.

TEXT

1. Introduction

Nanotechnology has the potential to revolutionize numerous aspects of our daily life. Engineered nanomaterials (NMs) have become technological and economic stakes for a wide range of applications, such as construction, plastic processing, fabrics, and energy. The biological applications of NMs are expanding in food industry, cosmetics, pharmacology and medicine, covering a number of different uses from antimicrobial coating and targeted drug delivery to material biocompatibility and imaging. In particular, the rapid growth of nanomedicine has seen a large set of NMs being investigated to evaluate their potential as drug carriers, vaccine adjuvants, biocompatible implants or diagnostic probes. The number of products containing NMs has been multiplied by five between 2006 and 2011 and over 1800 products containing NMs have been produced in 2014.

Simultaneously, the field of nanotoxicology has significantly developed to investigate the risks and the impacts of NM exposure on the environment and health. The assessment of NM toxicity has involved substantial evolutions in the field to deal with the specific interactions of NMs with biological systems. The understanding of the formation of the protein corona and its key role as an interface between biological systems and NMs has been an essential step.
Indeed, the adsorption of biomolecules on the surface of NMs in the biological medium leads to the formation of a complex and dynamic corona, giving NMs their ‘biological identity’ \(^{27,28}\). The protein corona determines the NM uptake and its biological outcome \(^{29-31}\). Moreover, the control of the conformation and the activity of the adsorbed proteins is necessary to achieve good material biocompatibility \(^{32,33}\). A better understanding of the molecular interactions between NMs, defined by their physical and chemical properties, and endogenous proteins likely to adsorb on the surface is thus essential to study and predict their biological effects and to design NMs with excellent biocompatibility \(^{34,35}\).

It has been known for a long time that protein adsorption on flat surfaces can result in a modification of the protein structure and activity \(^{36,37}\). Similarly, protein adsorption on NMs can impair protein structure and function \(^{38,39}\). The control of the protein functional state is particularly important when designing hemoglobin-loaded nanoparticles as blood substitutes \(^{40}\). However, the relationship between the NM properties and the adsorbed protein structure, dynamics and activity is still poorly understood. Based on the adsorption of model proteins on hydrophobic and hydrophilic particles, Norde and co-workers developed a model to predict protein adsorption as a function of protein charge and structural stability \(^{41,42}\). According to this model, adsorption on a hydrophilic surface is driven by electrostatic forces and the structural modifications of the adsorbed proteins. Structural rearrangements would significantly contribute to the adsorption of ‘soft proteins’ with a lower internal stability compared to ‘hard proteins’ with a strong internal stability \(^{36,37}\). The main interactions and driving forces of protein adsorption were described by Czeslik \(^{43}\). More recently, we have developed a strategy to determine the physico-chemical determinants of protein adsorption based on the identification of the adsorbed and non-adsorbed proteins in a mixture of hundreds of proteins, and on the
statistical comparison of the structural features of each group. This approach revealed the molecular bases of protein adsorption on silica nanoparticles (SNPs), that is an enrichment in basic residues (particularly Arg) and a low content in aromatic residues (Phe, Trp, Tyr, and His). The protein adsorption is thus correlated to the protein flexibility and ability to spread on the surface.

Protein adsorption on nanoparticles is often associated to a partial loss of secondary structure, even if helix formation has also been observed in some cases. The structural modifications depend on the size, shape and surface chemistry of the NMs. Moreover, protein adsorption can be used to promote enzyme stability in bioreactors and biosensors for industrial applications. The enzymatic activity can be decreased, increased or can remain constant after adsorption, highlighting the complex relationship between the structural and the functional modifications of adsorbed proteins. In Norde’s model, structural rearrangement contributes to protein adsorption by leading to an increase of the degree of freedom of the polypeptide chain and finally to an increase in protein flexibility. In this model, the protein structure loss would lead to a favourable gain in entropy. However, few experimental studies have been performed to investigate protein dynamics on surfaces despite its importance in biological processes. Recent studies rather suggest that protein adsorption can result in a decrease of the adsorbed protein dynamics. Using elastic and inelastic neutron scattering experiments, we showed that myoglobin adsorption on SNPs leads to a decrease of protein flexibility and to a depletion in low frequency modes, suggesting that the structural loss of the adsorbed protein may not be the entropic driving force of adsorption. The aim of this study is to investigate the modifications of hemoglobin structure and activity after adsorption on SNPs in connection with our results on the dynamics of adsorbed myoglobin.
SNPs are produced and used at an industrial scale, especially in food products. In this study, we used SNPs as a model hydrophilic inorganic surface. Hemoglobin and myoglobin belong to the same family of hemoproteins. Hemoglobin has several advantages as a model protein: its biochemical and structural properties are well characterized; and its function of oxygen binding is particularly well suited to study its activity after adsorption. Indeed, it does not involve any substrate or cofactor that may interact with the SNPs during the reaction, contrary to most enzymatic reactions, preventing any interference during the experimental measurement of the protein activity. We investigated the mechanisms of hemoglobin adsorption on SNPs and we analysed the effect of the structural rearrangement on the surface on the activity of hemoglobin. Our results suggest that adsorption leads to a new state characterized by specific structural and functional features with full reversibility, in a way that significantly differs from protein denaturation.

2. Methods

Hemoglobin. Porcine hemoglobin (Sus scrofa domesticus) was purified in the oxygenated form (HbO₂) from fresh blood following standard preparation using erythrocyte membrane precipitation in 0.28 M Phosphate pH 7.0. HbO₂ solution was extensively dialyzed against pure water at 4°C, stripped by passing hemoglobin desalted solution through a mixed-bed ion-exchange resin (AG 501-X8 from Bio-Rad) to remove naturally bound 2,3-diphosphoglycerate (DPG) and centrifuged at 20,000 g for 10 min. HbO₂ concentration expressed as heme molar concentration was measured on a Shimadzu UV-2450 spectrophotometer taking ε₅₇₆ nm = 15,150 M⁻¹.cm⁻¹. Possible iron oxidation and potential protein damages were systematically screened by measuring the absorbance ratio at 576 nm and 541 nm.
**Chemicals.** BisTris-HCl, Tris-HCl and Phosphate buffers were prepared at a concentration of 0.1 M by dissolution of BisTris (Sigma-Aldrich B9754), Tris (Sigma-Aldrich T6066), monosodium phosphate (Sigma-Aldrich 71649) and disodium phosphate (Fisher Scientific S3720). 2,3-diphosphoglycerate (DPG) (Sigma-Aldrich D5764) and inositol hexaphosphate (IHP) (Sigma-Aldrich P0109) were dissolved in 0.1 M BisTris-HCl pH 6.0. To avoid DPG hydrolysis, a fresh solution was prepared before each oxygen binding experiment.

**Silica nanoparticles.** As explained in the introduction, SNPs (Sigma-Aldrich 637238) come from the same batch as in our previous studies \(^4^4\) and were extensively characterized. Their mean diameter is 26 ± 2 nm and their surface area is 170 m\(^2\)/g. SNPs were suspended in buffered solutions and vortexed for 1 min. Small aggregates of 50 ± 2 nm formed in solution.

\(\zeta\)-potential. Zeta potential (\(\zeta\)) of SNPs was measured at 25°C on a Zetasizer Nano-ZS (Malvern Instruments) in 0.1 M BisTris-HCl pH 6.0, Phosphate pH 7.4 and Tris-HCl pH 8.7. SNP concentration is 0.1 mg/mL. Each measurement was repeated 5 times. The \(\zeta\)-potential was calculated by fitting the electrophoretic mobility with the Smoluchowski model.

**Adsorption isotherms and protein desorption.** Adsorption isotherms of HbO\(_2\) on SNPs were measured by the depletion method \(^4^7\). HbO\(_2\) solution was added to SNP suspension with a final SNP concentration of 4.5 mg/mL and smoothly mixed overnight at 20°C. The sample was then centrifuged at 20,000 g for 10 min. HbO\(_2\) concentration in the supernatant was measured by spectrophotometry. The amount of adsorbed protein is expressed as mg/m\(^2\). An uncertainty of 5% on the amount of adsorbed protein was determined by repeating 5 times this procedure. Protein desorption was measured after incubation of 50 µM HbO\(_2\) with SNPs at a concentration of 34 mg/mL overnight. The solution was centrifuged at 20,000 g for 10 min and the supernatant removed. The SNPs were resuspended in the leaching solution by smooth mixing at 20°C, before
centrifugation at 20,000 g for 10 min and measurement of HbO$_2$ concentration in the supernatant. To avoid harsh pH change when adding the leaching solution, an additional experiment was performed by dialysis in 0.1 M Tris-HCl buffer at pH 8.7 at 4°C overnight using a Spectra/Por membrane with a 50 kDa cut-off. All the measurements were done in triplicate.

Structural analysis. UV-visible spectra were recorded in 1-cm path length quartz cell from 250 to 800 nm at 25°C on a Shimadzu UV-2450 spectrophotometer equipped with an integrating sphere module. Circular dichroism spectra were recorded from 190 to 260 nm in 1-mm path length cell at 25°C on a Jobin-Yvon CD6 dichrograph. To minimize UV absorption by the buffers, HbO$_2$ spectra were recorded in 0.01 M BisTris-HCl, Tris-HCl and Phosphate. Final HbO$_2$ concentration was 10 µM and SNP concentration was 6.8 mg/mL. Each spectrum is the average of 4 measurements after baseline correction. The CD spectra of the solutions containing HbO$_2$ and SNPs were baseline corrected with the SNP solution. However, no signal was recorded for SNP solutions in these conditions. To control that no particle deposition occurred during the measurement, the absorbance at 280 nm was recorded before and after the acquisition of the CD spectrum. No evolution was observed. The alpha-helical content $f_\alpha$ was first determined from the ellipticity value at 222 nm according to eq. 1.

$$f_\alpha = \Delta\varepsilon(222 \text{ nm}) \cdot \frac{2340}{30300} \quad \text{(eq. 1)}$$

The circular dichroism spectra were then fully deconvoluted using CDNN software (Applied Physics). All the CD analyses were done in triplicate and a single representative spectrum corresponding to one sample scanned 4 times is shown.

Oxygen binding curves. HbO$_2$ at a concentration of 50 µM was smoothly mixed overnight with SNPs at a concentration of 34 mg/mL in 0.1 M BisTris-HCl, Tris-HCl or Phosphate. Oxygen binding was measured in a tonometer by spectrophotometry at 25°C and at 37°C. HbO$_2$ was
deoxygenated under an argon flow that bubbled in pure water to prevent drying. Oxygen binding was recorded by following the absorption at 576 nm. No desorption of hemoglobin from SNPs was observed during deoxygenation at pH 6.0 and at pH 7.4. All the measurements were done in triplicate.

3. Results

3.1 Monitoring HbO$_2$ adsorption with pH

The adsorption of hemoglobin on SNPs was quantified by the depletion method where the concentration of free protein is measured in the supernatant. However, the red color of HbO$_2$ allows for the direct observation of protein adsorption (Fig. 1A). Indeed, two markedly different behaviors were observed. The red pellet and transparent supernatant indicate strong protein adsorption in BisTris-HCl at pH 6.0, whereas the white pellet and red supernatant indicate little or no adsorption in Tris-HCl at pH 8.7. This observation was further confirmed by the measurement of the adsorption isotherms in BisTris-HCl pH 6.0, in Phosphate pH 7.4 and in Tris-HCl pH 8.7 (Fig. 1B). The maximum amount of adsorbed HbO$_2$, $m_{ads}$, is high at pH 6.0 ($m_{ads} = 0.41 \pm 0.02$ mg/m$^2$) and at pH 7.4 ($m_{ads} = 0.34 \pm 0.02$ mg/m$^2$), and null at pH 8.7.
Figure 1. Adsorption behavior of HbO$_2$ on SNPs. A) Images, after centrifugation, of HbO$_2$ solution mixed with SNPs in 0.1 M BisTris-HCl pH 6.0 or Tris-HCl pH 8.7; B) Adsorption isotherms of HbO$_2$ on SNPs in 0.1 M BisTris-HCl pH 6.0 (circle), Phosphate pH 7.4 (square) and Tris-HCl pH 8.7 (triangle). Fitting by the Langmuir model is represented by solid lines.

The adsorption constant $K_{ads}$ which reflects the affinity of the protein for the surface was calculated by fitting the adsorption isotherms with the Langmuir model according to eq. 2 (Fig. 1B).

$$m_{ads} = \frac{m_{\infty} \cdot K_{ads} \cdot C}{1 + K_{ads} \cdot C} \quad \text{(eq. 2)}$$

Where $C$ is the protein concentration at equilibrium and $m_{\infty}$ the maximum amount of adsorbed protein. The Langmuir equation is valid for the reversible adsorption of a monolayer of non-interacting molecules on a surface with identical binding sites. Since protein adsorption often results in irreversible binding to the surface, the validity of the Langmuir model to depict protein
adsorption has been discussed in the literature. In the case of hemoglobin, the plateau value clearly indicates monolayer adsorption on the surface (see §3.5).

The very different adsorption behavior at pH 6.0 and at pH 8.7 suggests a strong effect of charges on the adsorption of HbO2 on SNPs. The surface chemistry of amorphous SNPs in aqueous solution is characterized by the hydroxylation of the surface leading to a surface coverage by silanol groups (Si-OH) of 4.6-4.9 OH/nm². The extent of ionization of the silanol groups in siloxide (Si-O⁻) that gives its negative charge to SNPs at neutral pH depends on the size of the particles and on the ionic strength. The surface charge density increases when SNP size decreases and when the ionic strength increases. In our study, the negative charge of SNPs in the different buffers was confirmed by measuring the ζ-potential of the particles highlighting the increase in surface charge density with pH (Table S1).

The adsorption behavior of hemoglobin on SNPs as a function of pH was further investigated by measuring the adsorption isotherms from pH 6.0 to 7.8 in BisTris-HCl, from pH 7.0 to 7.8 in Phosphate and from pH 7.2 to 8.7 in Tris-HCl (Fig. 2A). The porcine HbO₂ tetramer is structurally similar to that of human oxyhemoglobin and its global isoelectric point is around 7.2. The amount of adsorbed HbO₂ represented for each condition in Fig. 2B reveals a maximum level of adsorption from pH 6.2 to pH 7.3 both in BisTris-HCl and Tris-HCl, followed by a sharp decrease from pH 7.3 to pH 8.5 until zero adsorption. We can notice that for pH > 7.2, the adsorption isotherms do not reach a plateau in this concentration range. Thus, the maximum amount of adsorbed HbO₂ indicated in Fig. 2B corresponds to the value of the last point of the adsorption isotherm represented in Fig. 2A and may be underestimated. Alternative models may represent better fit of the adsorption isotherms in these conditions, as suggested by Findenegg and coworkers. No buffer effect was observed for BisTris-HCl and Tris-HCl although a little
effect was observed for Phosphate for which slightly lower amounts of HbO₂ adsorbed in the same pH conditions.

Figure 2. Control of HbO₂ adsorption on SNPs by pH. A) Adsorption isotherms of HbO₂ on SNPs in 0.1 M Tris-HCl from pH 7.2 to 8.7; B) Maximum amount of adsorbed HbO₂ on SNPs in 0.1 M BisTris-HCl (circle), Phosphate (square) and Tris-HCl (triangle) at different pH.

The affinity of HbO₂ for SNPs decreases as pH increases as shown by the decrease of $K_{ads}$ from pH ≥ 7 (Table 1). The adsorption of HbO₂ on SNPs is thus favored when the protein is globally positively charged or neutral (pH ≤ 7.2) and becomes less and less favorable with the increase of HbO₂ and SNP negative charges (pH > 7.3) until charge repulsion completely prevents protein adsorption (pH ≥ 8.5). Indeed, the electrostatic interactions between the anionic siloxide groups
and the basic amino acids (Lys, Arg) are known to play a key role in protein adsorption on SNPs especially when the basic residues form positively charged clusters in the protein structure. Hemoglobin α chains and β chains contain 14 basic residues (11 Lys, 3 Arg) and 16 basic residues (11 Lys, 5 Arg) respectively. It suggests that both subunits could contribute to the electrostatic interactions responsible for HbO₂ adsorption and non-adsorption to SNPs. At the same pH, $K_{ads}$ is smaller for Phosphate compared to BisTris-HCl or Tris-HCl, suggesting that ion pairing and ion replacement also play a role in HbO₂ adsorption on silica.

<table>
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<td>-</td>
<td>-</td>
</tr>
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<td>-</td>
</tr>
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</tr>
<tr>
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<td>8.1</td>
<td>-</td>
<td>-</td>
<td>0.05 $10^6$</td>
</tr>
</tbody>
</table>

Table 1. Adsorption constant $K_{ads}$ (M⁻¹) of HbO₂ on SNPs in 0.1 M BisTris-HCl, Phosphate and Tris-HCl.

We can conclude that HbO₂ adsorption on SNPs is primarily driven by pH with a minor effect of the ions in solution. HbO₂ adsorption can be fully controlled in a small pH range, independently of the total protein concentration in solution, from a maximum protein coverage at pH 7.3 to no protein adsorption at pH 8.5.

### 3.2 Structural analysis of adsorbed HbO₂

The structure of HbO₂ adsorbed on SNPs was investigated by circular dichroism (CD) (Fig. 3) and by UV-visible spectroscopy (Fig. S1) to analyze the protein secondary structure and the oxygenated heme electronic structure respectively. A concentration of 10 µM HbO₂ and 6.8 mg/mL SNPs were chosen to achieve almost complete protein adsorption. The amount of adsorbed HbO₂ in this condition is 99% at pH 6.0, 90% at pH 7.4 and <1% at pH 8.7 (Table S2).
The spectra measured at pH 6.0 and at pH 7.4 can thus be attributed to the adsorbed protein with no contribution or little contribution from the free protein in solution at pH 6.0 and at pH 7.4 respectively. As SNPs may interfere with the optical measurement, a control experiment was systematically performed to compare the spectra of free HbO2 with SNPs and native HbO2 without SNPs, both in Tris-HCl at pH 8.7. Indeed, no adsorption occurs in this condition so that any change in the protein spectrum would indicate a bias due to the particles in suspension. The CD spectra of free and native HbO2 measured at pH 8.7 with and without SNPs respectively (Fig. 3C) are identical showing that no protein structure perturbation arises from SNPs in suspension.

The CD spectra of adsorbed HbO2 at pH 6.0 (Fig. 3A) and at pH 7.4 (Fig. 3B) showed a decrease in |Δε| compared to native HbO2 indicating a modification of the secondary structure after adsorption on SNPs. The spectrum of native HbO2 is characterized by one maximum at 192 nm and two minima at 208 nm and 222 nm corresponding to the predominant α-helix secondary structure. As reported before, the secondary structure of HbO2 is identical at pH 6.0, at pH 7.4 and at pH 8.7 in the different buffers. The percentage of α-helix calculated from the ellipticity at 222 nm decreases from 80% for native HbO2 to 62% and 49% for adsorbed HbO2 at pH 7.4 and at pH 6.0 respectively. The helicity calculated for adsorbed HbO2 at pH 7.4 was corrected from the contribution of free HbO2 in solution.

Spectral deconvolution by CDNN confirmed the important loss of α-helix structure together with an increase in random coil up to 17% at pH 6.0. Therefore HbO2 molecule loses a significant part of its helical secondary structure after adsorption on SNPs with a gain of disordered regions, similarly to HbO2 adsorption on quantum dots and on silver nanoparticles. Though the formation of some β-sheet cannot be excluded, it has also been shown that a
change in the \( \Delta \varepsilon \) ratio at 222 nm and 208 nm of \( \alpha \)-helical proteins can be related to intra- and inter-molecular helix interactions and coiled-coil formation which could be indicative of a modification of adsorbed hemoglobin tertiary structure \(^{77}\).
**Figure 3. Circular dichroism spectra of adsorbed HbO\(_2\) on SNPs.** HbO\(_2\) with (red) and without SNPs (blue) in BisTris-HCl pH 6.0 (A), Phosphate pH 7.4 (B) and Tris-HCl pH 8.7 (C). The heme group, which is the active site of hemoglobin molecule, is composed of a porphyrin ring with an iron atom at its center allowing oxygen binding. The electronic structure of the heme group was probed by UV-visible spectroscopy. An integrated sphere module was used to collect the light scattered by SNPs allowing the measurement of quality spectra of HbO\(_2\) in the 250-700 nm range with SNPs (Fig. S1). As expected, the spectra of HbO\(_2\) obtained without SNPs are independent of pH in the range of protein stability\(^{60}\).

In the control spectrum measured at pH 8.7 with SNPs, no shift of the characteristic absorption peaks of HbO\(_2\) and no absorption change of the Soret band at 414 nm and of the Q bands at 541 and 576 nm that correspond to electronic transitions in the heme group [55] was observed (Fig. S1). A slightly higher absorption measured in the 250-400 nm range in all pH conditions indicates that light scattering by SNPs is not fully corrected below 400 nm. The spectra of adsorbed HbO\(_2\) at pH 6.0 and at pH 7.4 are identical to the spectrum of HbO\(_2\) at pH 8.7 indicating that adsorption on SNPs does not lead to any major modification of the heme electronic structure. Despite the large change of oxyhemoglobin secondary structure, the heme group is not altered by adsorption on SNPs.

The activity of hemoglobin does not depend solely on the heme group and is strongly affected by the globin structure and dynamics\(^{78}\). The tetrameric structure of hemoglobin is central to the cooperative binding of oxygen\(^{79}\). However, the quaternary structure of adsorbed oligomeric proteins remains a blind spot in most cases. We investigated the oxygen binding activity of adsorbed hemoglobin to gain a full picture on the oligomerization state of adsorbed hemoglobin on SNPs.
3.3 Functional analysis of adsorbed hemoglobin

Oxygen binding curves of hemoglobin were measured in BisTris-HCl pH 6.0, Phosphate pH 7.4 and Tris-HCl pH 8.7 at 25°C (Fig. 4). Their sigmoidal shape reflects the cooperative binding of oxygen by tetrameric hemoglobin. The variation in hemoglobin affinity for oxygen with pH reflects the effect of bound or released protons by hemoglobin on its activity known as the Bohr effect. Both effects are quantified by the Hill coefficient ($n$) and the oxygen partial pressure at half saturation ($P_{50}$) determined by fitting the experimental curves with the Hill equation (eq. 3), where $Y$ is the fraction of oxyhemoglobin and $P_{O2}$ the oxygen partial pressure (Table 2).

$$\log \frac{Y}{1-Y} = n \cdot \log P_{O2} - \log P_{50} \quad (eq. \ 3)$$

No difference between the oxygen binding curves of hemoglobin at pH 8.7 with and without SNPs was observed confirming that SNPs did not interfere with oxygen binding or with the spectroscopic measurement (Fig. 4C). Fig. 4A and Fig. 4B exhibit a more hyperbolic shape of the oxygen binding curves. This significant increase of the affinity of adsorbed hemoglobin follows the decrease in cooperativity as shown by the decrease of $P_{50}$ from $17.1 \pm 0.5$ to $8.7 \pm 0.5$ mmHg at pH 6.0 and from $7.7 \pm 0.5$ to $4.7 \pm 0.5$ mmHg at pH 7.4. However, adsorbed hemoglobin still experience cooperative binding as evidenced by the Hill coefficients of $1.6 \pm 0.1$ and $1.9 \pm 0.1$ at pH 6.0 and pH 7.4 respectively. This cooperative behavior cancels the possibility of a dissociation of the tetramer into dimers or monomers during adsorption on SNPs.

<table>
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<th>pH</th>
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<th>$n$</th>
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<tr>
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Table 2. Oxygen partial pressure at half saturation (P$_{50}$) and Hill coefficient (n) of hemoglobin oxygen binding in 0.1 M BisTris-HCl pH 6.0, Phosphate pH 7.4 and Tris-HCl pH 8.7 at 25°C with and without SNPs. Values are given with an uncertainty of ± 0.5 mmHg (P$_{50}$) and ± 0.1 (n).
Figure 4. Effect of SNPs on hemoglobin activity. Oxygen binding curves of hemoglobin with (red) and without (blue) SNPs in BisTris-HCl pH 6.0 (A), Phosphate pH 7.4 (B) and Tris-HCl pH 8.7 (C). Black line represents fitting by the Hill equation.
We also investigated the effect of temperature on the activity of adsorbed hemoglobin on SNPs. The oxygen binding curves measured at 37°C at pH 6 and at pH 7.4 (Fig. S2) show a clear increase in oxygen affinity and decrease in cooperativity due to hemoglobin adsorption on SNPs in addition to the sole effect of temperature on hemoglobin activity (Table S3). Therefore, all the features observed at 25°C after adsorption on SNPs are preserved at 37°C in physiological conditions.

3.4 Binding of heterotropic effectors to adsorbed hemoglobin

Heterotropic effectors such as inositol hexaphosphate (IHP) and 2,3-diphosphoglycerate (DPG) have well-defined binding sites in the tetrameric protein. DPG is a natural effector of hemoglobin present in red blood cells at a concentration of 6 mM. It binds to hemoglobin, decreases hemoglobin oxygen affinity and eases oxygen release in tissues. Since adsorption of hemoglobin on SNPs increases hemoglobin affinity, we tested whether this effect could be counterbalanced by the addition of DPG. A second effector, IHP, which has the same binding site as DPG\textsuperscript{83} induces a larger decrease of hemoglobin affinity was also tested. DPG and IHP are both composed of negatively charged inorganic phosphate groups. The oxygen binding curves of adsorbed hemoglobin were measured with DPG or IHP in BisTris-HCl pH 6.0 (Fig. 5). The effector was added either before or after hemoglobin adsorption on SNPs to probe the accessibility and the structural integrity of the effector binding site after adsorption.

The affinity of native hemoglobin significantly decreased after addition of DPG or IHP with an increase of $P_{50}$ by a factor 2 after addition of DPG (38.5 ± 0.5 mmHg) and by a factor 6 after addition of IHP (110 ± 1 mmHg). Hemoglobin cooperativity was maintained after binding of DPG ($n = 2.8 ± 0.1$) but decreased after binding of IHP ($n = 2.2 ± 0.1$). We checked that there was no pH change after addition of an excess of DPG or IHP to the buffered solutions.
Figure 5. Effect of DPG and IHP effectors on adsorbed hemoglobin activity. Oxygen binding curves of native hemoglobin (circle) and adsorbed hemoglobin (triangle and square) with DPG (A) or with IHP (B) in 0.1 M BisTris-HCl pH 6.0 at 25°C. DPG or IHP were added either before (triangle) or after (square) adsorption of HbO$_2$ on silica NPs. Fitting by Hill equation is represented by a black line. Hemoglobin concentration is 50 µM, SNP concentration is 34 mg/mL, DPG and IHP concentration is 125 µM.

The affinity of adsorbed hemoglobin significantly decreased after addition of DPG (22.0 ± 0.5 mmHg) or IHP (104 ± 1 mmHg) compared to adsorbed hemoglobin without effectors (8.7 ± 0.5 mmHg). It shows that both effectors can efficiently shift adsorbed hemoglobin affinity towards lower values (Table 3). Interestingly, the oxygen binding curve of adsorbed hemoglobin with IHP is identical to the one of native hemoglobin with IHP (Fig. 5B), whereas the oxygen binding...
The oxygen binding curves of adsorbed hemoglobin are identical whether the effector was added before or after adsorption on SNPs. It clearly indicates that (i) DPG and IHP binding site is preserved and accessible after protein adsorption, and (ii) binding of the effector does not prevent adsorption on SNPs.

These results highlight the possibility of tuning hemoglobin activity to lower or higher affinity at will via a combination of pH and temperature values, binding of heterotropic effectors as DPG or IHP and adsorption on SNPs. From this point of view, silica nanoparticles may be considered as
a novel positive heterotropic effector of hemoglobin leading to a specific structural and functional state.

3.5 Reversibility of the structural and functional modifications of absorbed HbO₂

Desorption of HbO₂ from SNPs was tested in different conditions starting from adsorbed HbO₂ in BisTris-HCl pH 6.0 or in Phosphate pH 7.4 (Table S4). The SNPs were centrifuged and resuspended in a new solution. No desorption was observed in water, NaCl 1M, CaCl₂ 1M, BisTris-HCl pH 6.0 or Phosphate pH 7.4. It means that HbO₂ cannot be desorbed by dilution, ion exchange or washing. On the contrary, almost complete desorption was observed in Tris-HCl at pH 8.7 after 1h mixing or in softer conditions by dialysis overnight, with up to 90% of the adsorbed protein released in the solution. This result confirms the key role of electrostatic interactions in HbO₂ adsorption on SNPs and it provides a useful tool to study the reversibility of the structural and functional modifications of adsorbed HbO₂.

![Figure 6. Functional analysis of desorbed hemoglobin. Oxygen binding curves of native (circle) and desorbed (diamond) hemoglobin in 0.1 M Tris-HCl pH 8.7. Fitting by Hill equation is represented by a black line.](image-url)

We analyzed the structure and the function of HbO₂ desorbed from SNPs by dialysis in 0.01 M Tris-HCl pH 8.7. The UV-vis and CD spectra of desorbed HbO₂ are almost identical to the
spectra of native HbO\(_2\) (Fig. S3) indicating almost full reversibility of the structural modifications after desorption. The slight difference observed in CD spectra may indicate some remaining secondary and/or tertiary structural modifications \(^{77,84}\).

The analysis of the oxygen binding curves of desorbed hemoglobin (Fig. 6) confirmed that desorbed hemoglobin regained its native activity. Thus oxyhemoglobin can switch from one structural and functional state to another following an adsorption/desorption cycle in a reversible manner. This result indicates that adsorption of HbO\(_2\) on SNPs represents a highly tunable system in which the adsorption/desorption of the protein can be fully controlled by simple pH change.

4. Discussion

**Molecular mechanisms of HbO\(_2\) adsorption on SNPs**

Electrostatic interactions play a key role in HbO\(_2\) adsorption on SNPs as evidenced by the control of adsorption and the adsorption/desorption cycle as a function of pH. This is in agreement with the previous observation by Kondo *et al* of hemoglobin adsorption on ultrafine silica particles \(^{85}\). The electrostatic interactions between the basic residues and the siloxide groups can counterbalance the loss of H-bonding due to the large loss of the secondary structure in the enthalpic budget \(^{47}\). However, other interactions can possibly contribute to HbO\(_2\) adsorption such as polar interactions and H-bond formation \(^{43}\). In particular, H-bonds between silanol groups and the imidazole ring of His residue are known to favor peptide interaction with silica and to participate in silica biomineralisation *in vivo* \(^{86}\). The molecular mechanisms of protein adsorption on the same silica NPs were identified in our previous study on a larger protein population \(^{44}\). The structural determinants are the electrostatic interactions between clusters of basic residues (in particular Arg) and the silanol groups on one hand, and protein
flexibility associated to a low content of aromatic residues and π-π interactions on the other hand. Moreover, clusters of basic residues have also been identified in the binding sites of myoglobin on silica NPs, a hemoprotein which has a similar primary and secondary structure as hemoglobin. Desorption of HbO\(_2\) at pH 8.7 is likely due to electrostatic repulsion which can result from the deprotonation of silanol groups on the silica surface (surface charging), and/or from the deprotonation of Arg and Lys residues (loss of positive charges) (Fig. 7). Even though the pK\(_a\) of the side chain of the free basic amino acid is 12.0 and 10.4 respectively, it can widely vary inside the protein structure suggesting that some residues may already be deprotonated at pH 8.7. 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The hydration layer plays an important role in the adsorption of biomolecules on inorganic surfaces. From an energetic point of view, the displacement of water molecules from the silica surface can contribute to the adsorption of proteins on SNPs by the entropic gain associated to the release of water molecules from the surface. Water structure at the silica surface depends on the protonation state of the silanol groups. The orientation of water molecules, e.g. pointing towards the silica surface or towards the bulk, follows the formation of H-bonds either with the oxygen atom of the charged Si-O\(^-\) groups, or with the oxygen or hydrogen atoms of the neutral Si-OH group. A large number of deprotonated charged groups at higher pH also creates an electric field that contributes to water molecule orientation by charge-dipole interaction in the electric double layer. Thus, the surface properties to consider to describe protein adsorption on SNPs at a molecular level include the structure and protonation state of the silanol groups, the water structure and H-bond network at the interface and the effect of ions on the surface charge density. A description at a molecular level of the interactions between proteins and nanoparticles could help to further rationalize and control protein adsorption.
Interestingly, adsorbed hemoglobin is still responsive to the Bohr effect in a similar extent as native hemoglobin with a $P_{50}$ divided by two from pH 6.0 to pH 7.4. It indicates that the proton binding sites involved in this pH range are not affected by the adsorption on SNPs. However, their position in hemoglobin structure is not well defined because of the large number of possible residues. For example, hemoglobin tetramer counts 38 histidine residues which all have various pK$_a$ depending on their local environment and the protonation state of the other residues $^{91}$.

**Reorganization of the secondary structure of the adsorbed protein**

The significant loss of the helical structure means that the H-bond network that holds the protein secondary structure is destabilized during adsorption on SNPs. The difference in structural modification at pH 6.0 and at pH 7.4 is likely due to the lower affinity of HbO$_2$ for the silica surface at pH 7.4 where the molecular interactions, in particular the electrostatic interactions between basic amino acids and siloxide groups, may be fewer and/or weaker, resulting in less constraints on the adsorbed protein structure.

CD analysis does not allow to identify the protein domains affected by the loss of secondary structure and to decipher between a *short-range effect* due to the direct interaction between one or several residues involved in an α-helix and the SNPs surface; and/or a *long-range effect* $^{91}$ whereby α-helices which are not in close contact with the surface could be destabilized due to the global reorganization of the protein structure after adsorption. Indeed, if HbO$_2$ is ‘anchored’ on the silica surface through strong electrostatic interactions between basic residues and negatively charged moieties, then mechanical stress could apply to domains that are not in direct contact with the surface. Moreover, the extent of the conformational changes of adsorbed hemoglobin increases with time $^{92}$ which suggests further structural reorganization of the adsorbed protein on the surface following the first interaction and binding step. Such nonlocal
effects would imply that the disordered regions of the proteins would not necessarily correspond to the sole protein binding sites on SNPs.

**Oligomeric state of adsorbed hemoglobin**

The binding site of DPG and IHP is in the cavity formed by the two β chains of deoxyhemoglobin and involves the interactions of the side chains of the residues Val1, His2, Lys82 and His143 with the negative charges of the phosphate groups of the effectors $^{93-95}$. Therefore, the binding of DPG or IHP to adsorbed hemoglobin evidenced by the decrease of the oxygen affinity confirms the tetrameric structure of adsorbed hemoglobin. Indeed, if binding of DPG or IHP to a hemoglobin dimer may be possible, the decrease in affinity is much lower $^{96}$. It also indicates that the cavity between β chains is fully accessible to small molecules after adsorption. Our conclusion differs from the study of Hallaway and coworkers who concluded that the increase of hemoglobin affinity after adsorption on a Cab-O-Sil surface was due to the dissociation into dimers $^{97}$.

The distinct effect of DPG and IHP on adsorbed hemoglobin activity remains an open question. The activity of the adsorbed protein is identical to the activity of native hemoglobin when IHP is bound. Moreover, the cooperativity of adsorbed hemoglobin bound to IHP ($n = 2.1 \pm 0.1$) is higher than the cooperativity of adsorbed hemoglobin without effector ($n = 1.6 \pm 0.1$). We checked the secondary structure of adsorbed HbO$_2$ in presence of IHP by circular dichroism. The CD spectra of adsorbed HbO$_2$ are identical with and without IHP (Fig. S4) with an important loss of the helical structure after adsorption on SNPs. Thus, when adsorbed HbO$_2$ binds IHP, it retains a native activity despite the partial loss of its secondary structure.

**Relationship between structural and functional modifications of adsorbed HbO$_2$**
Contrary to denatured proteins, the significant loss of HbO$_2$ secondary structure does not induce a decrease of its activity but a large increase in oxygen binding affinity. Our results demonstrate that this effect can be rationalized by the preservation of the heme group and of the tetrameric structure of adsorbed HbO$_2$ with heme-heme interactions (Fig. 7). We can also notice that the loss of secondary structure is lesser than observed for heat or acidic denaturation of HbO$_2$.\textsuperscript{98}

Whereas the monomer of absorbed myoglobin has two binding sites for silica\textsuperscript{73}, the lack of structural information at a residue level on tetramer structure of adsorbed hemoglobin or on binding sites prevents deeper analysis. Yet the increase of adsorbed HbO$_2$ activity and the full reversibility of the structural and functional modifications suggest that the structural state of adsorbed hemoglobin is different from a denatured state. We previously investigated the dynamics of myoglobin on SNPs and showed that, contrary to Norde’s prediction, adsorption of myoglobin on SNPs resulted in a decrease in protein dynamics\textsuperscript{47}. This result suggests that a decrease in hemoglobin dynamics could also impact its oxygen binding activity.

**Figure 7.** Relationship between the adsorption mechanism on SNPs and the structural, functional and dynamic properties of hemoglobin. The value attributed to each criteria
indicates an increase, a decrease or a preservation of a structural or functional property compared to native hemoglobin. The decrease in adsorbed hemoglobin dynamics is based on the experimental results showing a decrease of myoglobin dynamics after adsorption on the SNPs \(^{47}\). Numerous models have been proposed to account for hemoglobin cooperativity, such as the allosteric model proposed by Monod, Wyman and Changeux \(^{99}\), the stereochemical model suggested by Perutz \(^{100}\) or the dynamic allosteric model submitted by Yonetani \(^{78}\) to cite only a few of them. Though the aim of this study is not to test the different models, we can discuss our experimental results on adsorbed hemoglobin structure/function/dynamics in line with the main models proposed.

In the sequential model of cooperativity based on Perutz hypothesis of two distinct quaternary structures of hemoglobin, the cooperative oxygen binding is explained by a switch from a low affinity form to a high affinity form \(^{100}\). We have demonstrated that hemoglobin tetrameric structure was preserved after adsorption on SNPs. Though further structural analysis would be necessary, our results do not support the idea that different quaternary structures are present and could afford for the increase in affinity of absorbed hemoglobin after a sequential mechanism (as that proposed by Perutz) given the large structure loss observed after adsorption.

According to Yonetani, thermic fluctuations of hemoglobin ease or prevent oxygen release from the heme through the globin, a higher dynamic resulting in a lower affinity of hemoglobin \(^{78,101}\). If we assume a decrease of adsorbed hemoglobin dynamics as suggested from the analysis of myoglobin dynamics \(^{47}\), then this model could possibly account for the increase in oxygen affinity.

Finally, the tunable adsorption and desorption of hemoglobin on SNPs with pH change, and the full control of hemoglobin activity by pH, temperature and the addition of inorganic phosphate
effectors opens the way to an interesting system whereby protein adsorption on nanoparticles can allow for full control over hemoglobin oxygen binding activity.

**Conclusion**

We investigated porcine hemoglobin adsorption on silica nanoparticles and we analyzed the structural and functional modifications of the adsorbed protein. HbO₂ adsorption can be controlled by pH from maximum adsorption between pH 6.0 and 7.0 to no adsorption at pH 8.5. The structural analysis of adsorbed HbO₂ on SNPs revealed a significant loss of secondary structure and a preservation of the heme oxidation state and environment. Despite the large secondary structure loss, adsorbed hemoglobin exhibited enhanced activity with a higher oxygen affinity and a lower cooperativity. The affinity of adsorbed hemoglobin could be further controlled by pH, temperature and the addition of inorganic phosphate effectors. The oxygen binding properties of adsorbed hemoglobin and its capacity to efficiently bind DPG and IHP effectors indicate that adsorbed hemoglobin retained its tetrameric structure. Moreover, the structural and functional modifications of adsorbed hemoglobin are fully reversible after complete desorption at pH 8.7.

Our results suggest that adsorption leads to a new state characterized by specific structural, functional and dynamic features with full reversibility in a way that significantly differs from protein denaturation. Finally, silica nanoparticles may be considered as a new and alternative positive effector for hemoglobin.

**ASSOCIATED CONTENT**

Zeta potential of SNPs; UV-visible spectra of HbO₂; oxygen binding curves at 37°C; structural analysis of desorbed HbO₂; structural analysis of HbO₂ bound to IHP.

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ABBREVIATIONS

SNP: silica nanoparticle; NM: nanomaterial; HbO₂: oxyhemoglobin; DPG: 2,3-diphosphoglycerate; IHP: inositol hexaphosphate.

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